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2	Evaporative heat loss insufficient to attain heat balance at rest in individuals with a spinal cord
3	injury at high ambient temperature
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27 Running head

28 Evaporative heat loss insufficient to attain heat balance

29 ABSTRACT

30 The aim of the study was to determine whether climatic limits for achieving heat balance at 31 rest are affected by spinal cord injury (SCI). Twenty-three males (8 able-bodied (AB), 8 with 32 paraplegia (PP) and 7 with tetraplegia (TP)) rested in 37°C and 20% relative humidity (RH) 33 for 20 mins. With the ambient temperature held constant, RH was increased by 5% every 7 34 mins, until gastrointestinal temperature (T_{gi}) showed a clear inflection or increased by >1°C. 35 T_{gi}, skin temperatures, perceptual responses and metabolic energy expenditure were measured 36 throughout. Metabolic heat production (AB: 123 (21) W, PP: 111 (15) W, TP: 103 (29) W) and 37 required rate of evaporative cooling for heat balance (Ereq, AB: 113 (20) W, PP: 107 (17) W, 38 TP: 106 (29) W) were similar between groups (p = 0.22 and p = 0.79). Compared to AB, greater 39 increases in T_{gi} were observed in TP (p = 0.01), with notable increases in mean skin temperature 40 (T_{sk}) for TP and PP (p = 0.01). A T_{gi} inflection point was demonstrated by 7 AB, only 3 out of 41 8 PP and none of TP. Despite metabolic heat production (and E_{req}) being similar between 42 groups evaporative heat loss was not large enough to obtain heat balance in TP, linked to a 43 shortfall in evaporative cooling potential. Although PP possess a greater sweating capacity, the 44 continual increase in T_{gi} and T_{sk}, in most PP, while lower than for TP, implies that latent heat loss for PP is also insufficient to attain heat balance. 45

46 NEW AND NOTEWORTHY

In the absence of convective heat loss, at temperatures around 37°C, evaporative heat loss is insufficient to attain heat balance at rest in individuals with paraplegia and tetraplegia. This finding was directly linked to a shortfall in evaporative cooling potential compared to required evaporative cooling. In this environment, both individuals with paraplegia and tetraplegia cannot subjectively determine the magnitude of their thermal strain, thus perceptual responsesshould not be relied upon for this population group.

53

54 Keywords: Tetraplegia, Paraplegia, Heat Balance, Passive Heat, Heat loss

55

56 INTRODUCTION

To prevent an accumulation of heat within the body and maintain a stable core temperature (T_{core}), individuals primarily rely on evaporative heat loss in warm and hot environments. Over a wide range of environments, T_{core} is able to equilibrate at levels proportional to metabolic rate known as the "prescriptive zone" (27), whilst being independent of ambient conditions. At thermal environments above this prescriptive zone T_{core} is forced out of equilibrium resulting in a continuous rise in T_{core} and the attainment of a critical environmental limit (23).

63

64 Individuals with a spinal cord injury (SCI) have a complete or partial loss of central control of 65 the sympathetic nervous system, resulting in a loss of sweating capacity and vasomotor control 66 below the lesion level. The higher the lesion level the smaller the body surface area of sensate 67 skin (14, 29) resulting in a reduction in sweating capacity and hence evaporative heat loss 68 potential. Most of the SCI literature investigating thermoregulation has involved exercise. 69 Although these studies, typically using upper body exercise, have not matched heat production 70 between groups, the premise of the exercise used within these studies was to replicate sporting 71 scenarios or provide an appropriate exercise stimulus for this population group (13, 33, 34). 72 However, to gain a deeper understanding of the effects an SCI has on heat dissipation, studies 73 need to be conducted at rest too (i.e. removing the additional metabolic heat production from 74 exercise), in environments considered compensable for the able-bodied (AB).

76 The lesion level of an individual with an SCI, determining the amount of remaining 77 sympathetic innervation, is likely to play an important role in the dissipation of heat through 78 sweating and the subsequent attainment of heat balance. An impairment or loss of motor and/or 79 sensory function of the cervical segments of the spinal cord results in tetraplegia (TP). 80 Whereas, an impairment or loss of motor and/or sensory function of the thoracic, lumbar or 81 sacral segments of the spinal cord results in paraplegia (PP). Both individuals with PP and TT 82 have a lower body surface area of sensate skin than AB individuals, with the amount of sensate 83 skin related to an individual's lesion level. Thus, TP have a lower body surface area of sensate 84 skin than PP. While all groups may be able to attain heat balance within a "prescriptive zone", 85 it is expected that PP and TP may reach a critical thermal environmental limit prior to AB, i.e. 86 a leftward shift in temperature and/or relative humidity (RH) of the prescriptive zone, with the 87 size of the shift related to their lesion level.

88

89 The aim of this study was to determine the effect the lesion level of an SCI has on the attainment 90 of a critical environmental limit. Experimental sessions were conducted at rest, in hot 91 conditions (37°C) using a stepwise increase in RH, based on the experimental design of previous studies (5, 21-23). The experimental design aimed to minimise heat loss from dry 92 93 heat loss by removing the skin to air temperature gradient and then progressively reducing the 94 water vapour pressure gradient from the skin to the environment, increasing the thermal stress 95 of the environment and hindering evaporative heat loss. Based on sweat rate capacity data from 96 pilot work, all groups were expected to have sufficient thermoregulatory capacity in the climate 97 chosen as the starting point of the protocol. It was hypothesised that critical environmental 98 limits would occur at high RH for AB. Whereas, in individuals with PP and TP it was 99 hypothesised that heat balance would be attained initially but a critical environmental limit would be reached prior to AB, with TP potentially experiencing a continual increase in T_{core}
from the early stages of the protocol.

102 MATERIALS AND METHODS

103 Participants. Twenty-three recreationally active male participants, consisting of eight AB 104 individuals, eight individuals with PP (T3-T12) and seven individuals with TP (C5/6-C6/7) 105 volunteered for the study. In PP, five had complete and three had incomplete injuries, whilst 106 in TP two had complete and five had incomplete injuries (Table 1). An individual with a 107 complete injury has no motor and/or sensory function preserved in the lowest sacral segments 108 of the spinal cord (S4-S5), whilst a motor or sensory incomplete injury refers to the 109 preservation of motor and/or sensory function in the lowest sacral segments (S4-S5, (24)). 110 Health and heat tolerance questionnaires were completed by all participants. All procedures 111 were approved by the University Ethical Advisory Committee and conformed to the 112 principles defined in the Declaration of Helsinki. Participants were fully informed of the 113 experimental protocols before providing written consent to participate.

114

Insert Table 1 here

Procedures. Participants were instructed to refrain from alcohol, caffeine and strenuous exercise 24 h prior to testing. All trials were conducted at the same time of day to negate circadian variation. Prior to arrival at the laboratory, participants ingested a telemetric pill (HQ Inc, Palmetto, Florida), for the measurement of gastrointestinal temperature (T_{gi}), 6-8 hours prior to experimental sessions to avoid the influence of ingested food or fluid on the temperature reading, in accordance with previous recommendations (6).

121

Upon arrival at the laboratory, skinfold measurements (Harpenden Skinfold Callipers, BatyInternational, West Sussex, UK) were taken from the biceps, triceps, subscapular and

124 suprailliac sites to calculate a sum of skinfolds (mm). Body fat percentage, using the Durnin 125 and Wormsley four site method, plus fat and fat free mass were calculated using age dependent 126 equations (9). To standardise clothing, all participants were given a pair of shorts and a short-127 sleeved t-shirt to wear during testing. Participants wore their own socks and sports shoes, with 128 an estimated clo value of 0.4 for the overall clothing ensemble (including wheelchair). Prior to 129 instrumentation, euhydration was confirmed for all participants (urine specific gravity <1.025, 130 Meta Scientific Ltd, Surrey, UK) and participants were weighed (Mettler Toledo KCC 150, 131 Leicester, UK, accuracy \pm 5g, resolution 1g) before entering the climatic chamber (T.I.S.S. 132 Peak Performance, Series 2009).

133

134 Skin temperature was measured throughout the protocol at 10 sites using iButtons (DS1922T, 135 Maxim Integrated Products, Inc., Sunnyvale, CA, USA), which were applied to the forehead 136 and on the right side of the body at the forearm, upper arm, chest, abdomen, upper back, thigh, 137 calf, hand and foot. Mean skin temperature (T_{sk}) was calculated in accordance with the formula 138 by Ramanathan (35).

139

140 During the protocol, PP and TP remained in their own daily wheelchair, whilst AB remained 141 seated in a similar wheelchair provided. The climatic chamber was initially set at 37°C and 142 20% RH (water vapour pressure in the ambient air $(P_a) = 1.26$ kPa). Participants were 143 informed that the RH would increase during the protocol but were not told the initial starting 144 RH or when the RH was being increased. Participants sat for an initial 20 min stabilisation 145 period, after which the RH was increased by 5% steps ($\Delta P_a = 0.314$ kPa) every 7 minutes, 146 whilst the ambient temperature was kept constant ($37.2^{\circ}C \pm 0.2^{\circ}C$ throughout all trials). By 147 the end of the 7 minutes the climatic chamber had just reached the desired humidity resulting in a steady ramp in humidity. Air velocity was measured as $0.12 \pm 0.07 \text{ m} \cdot \text{s}^{-1}$ throughout all 148

trials. Based on sweat rate capacity data from pilot work, all groups were expected to have sufficient thermoregulatory capacity during the stabilisation period. The ambient temperature and RH inside the climatic chamber were measured next to the participant (Testo 435, Testo AG, Germany). Participants were withdrawn from the climatic chamber after a clear inflection point in T_{gi} had been observed (critical RH limit, (26)), or T_{gi} increased by 1°C from the initial value upon entering the chamber (Figure 1).

155

Insert Figure 1

Heart rate (HR, Polar PE 4000, Kempele Finland) and T_{gi} were measured throughout. Perceptual measures of thermal comfort, thermal sensation and wetness sensation were taken during the last minute of each step increase in RH. The thermal sensation scale comprised of categories ranging from 0 ("unbearably cold") to 8 ("unbearably hot") in 0.5 increments (42). The thermal comfort scale ranged from 1 ("comfortable") to 4 ("very uncomfortable") in increments of 1 (12). The wetness sensation scale ranged from 0 ("dry") to 6 ("dripping wet") in increments of 1 (modified scale from (15)).

163 Fluid balance. Participants could drink water ad libitum, except during the last minute of each 164 7 min stage to prevent interference with respiratory measures. Fluid consumption was recorded 165 and was kept at the same temperature of the chamber to prevent any cooling effect of the fluid 166 on the participant. Upon removal from the climatic chamber and towel drying their skin, if 167 required, participants were re-weighed and provided another urine sample, which was analysed 168 for urine specific gravity. The towel was subsequently weighed and any sweat trapped in the 169 towel added to the participant's end weight. Sweat loss was adjusted for respiratory mass loss (Table 3). In addition to the percentage change in body mass ((Mass_{pre} - Mass_{post}) / 170 171 $Mass_{pre} \cdot 100$), the change in body mass adjusted for fluid consumed (total mass loss) was also 172 calculated ((Masspre - Masspost) + fluid consumed).

Ventilatory data and heat balance calculations. Expired gas was recorded continuously
throughout the test using a calibrated online gas analysis system in breath by breath mode
(Metamax, Cortex Biophysik GmbH, Leipzig, Germany). Saturated water vapour pressure
(P_{sa}), saturated skin vapour pressure (P_{sk}) and P_a were calculated using the following equations
(30).

$$P_{sa}(kPa) = \frac{e^{(18.956 - (4030.18 \div T_a + 235))}}{10} \tag{1}$$

$$P_{sk}(kPa) = \frac{e^{(18.956 - (4030.18 \div T_{sk} + 235))}}{10}$$
(2)

$$P_a(kPa) = (\Phi \cdot 0.01) \cdot P_{sa} \tag{3}$$

178 Where: T_a is the ambient temperature (°C) and Φ is the relative humidity.

179 Metabolic energy expenditure (M) was obtained from minute-average values for $\dot{V}O_2$ in litres 180 per minute and respiratory exchange ratio (RER) collected with the metabolic cart. Metabolic 181 energy expenditure was calculated using the equation below:

$$M(W) = V\dot{O}_2 \frac{\left(\frac{RER - 0.7 \cdot e_c}{0.3}\right) + \left(\frac{1 - RER \cdot e_f}{0.3}\right)}{60} \cdot 1000$$
(4)

182 Where: ec is the caloric equivalent per litre of oxygen for the oxidation of carbohydrates (21.13 183 kJ), and e_f is the caloric equivalent per litre of oxygen for the oxidation of fat (19.62 kJ). Since 184 the rate of external work (W) was assumed to be zero (i.e. any work on surrounding objects 185 was negligible), metabolic heat production (M-W) was taken to be equal to metabolic energy 186 expenditure. Dry heat exchange (radiative (R) and convective (C)), evaporative (E_{res}) and 187 convective respiratory heat exchange (C_{res}) and required rate of evaporative cooling (E_{req}) were 188 calculated using the following equations. Eres enabled the calculation of mass loss via the 189 respiratory system (M_{res}).

Dry (W) =
$$\frac{T_{sk} - T_a}{I_{cl} + \left(\frac{f_{cl}}{h_c + h_r}\right)} \cdot BSA$$
(5)
$$f_{cl} = 1.0 + 0.31 \cdot I_{cl}$$
(6)

$$C_{res} + E_{res} (W) = (0.0014 \cdot M \cdot (34 - T_a) + 0.0173 \cdot M \cdot (5.87 - P_a))$$
(7)

$$M_{res} (g \cdot h^{-1}) = E_{res} \cdot \frac{3600}{2430}$$
(8)

$$E_{reg}$$
 (W)= M - W - (C + R + C_{res} + E_{res}) (9)

190 Where: I_{cl} is the intrinsic clothing insulation (estimated to be 0.4 clo) and f_{cl} is the clothing area 191 factor, which is the ratio of the clothed surface area of the body to the nude surface area of the 192 body. h_c is the convective heat transfer coefficient (estimated at 3.1 W·m⁻² K⁻¹ when air velocity 193 is less than 0.2 m·s⁻¹), (28) and h_r is the radiative heat transfer coefficient (estimated at 4.7 194 W·m⁻² K⁻¹) for typical indoor conditions, (1). Body surface area (BSA) was calculated using 195 the Dubois formula (8).

196

Statistical analyses. All data were analysed using the Statistical Package for Social Sciences
(version 19, SPSS Chicago, IL) and are presented as mean (SD). An *a priori* power analysis,
conducted in G*Power 3.1, revealed a minimum sample size of 6 participants was required per

group, with 90% power and an α of 5%, based on findings from (31). Given the heterogeneity
of the population group, additional participants were recruited to increase statistical power.

202

203 Delta HR, Tgi, Tsk and individual skin temperatures were calculated as the change from the last 204 minute of the 20 min stabilisation period. Statistical analysis was conducted for repeated 205 measures up to 65% RH (n = 23), thereafter several participants from PP and TP were removed 206 due to $a \ge 1^{\circ}C$ change in T_{gi} or the participant had reached a critical RH limit. To account for 207 the reduced number of participants tested at 70-90% RH, predicted lines were calculated for the change in T_{gi} and T_{sk} to indicate the expected trend (Figure 2). To calculate the predicted 208 209 delta data the difference between each time point for each remaining individual were 210 calculated. The average differences for each time point were then added to the previous time 211 point to estimate data points for 70-90% RH where dropouts were present. For ventilatory data 212 and the heat balance calculations, data from two AB participants were excluded due to missing 213 data as a result of equipment error.

214

For all groups a critical RH was determined grapically from the raw data. A line was drawn between the data points of T_{gi} starting from an initial equilibirum phase. When the T_{gi} slope started to deviate upward from the equilibrium slope, a second line was drawn from the point of deviation from the first line. The RH before the point at which the second line deviated from the first was defined as the critical RH, a method previously used in (23).

Distribution and normality of data were assessed using the Shapiro–Wilk test. For data violating normality and homogeneity assumptions, logarithmic or square-root conversions were applied. For one way analysis of variance (ANOVA), if these conversions failed to correct the skew and heterogeneity, a Kruskal-Wallis test was used. To analyse any between group differences at both the start and at 65% RH a one way ANOVA was used, whilst for between 225 group differences during the protocol a mixed method ANOVA was used. Where significance 226 was obtained, post hoc pairwise comparisons with a Bonferroni correction were conducted. 227 Main effects and interactions were accepted as statistically significant when $p \le 0.05$. A main 228 effect of time corresponded to a step increase in RH. Confidence intervals (95% CI) for 229 differences are presented, alongside effect sizes (ES) to supplement significant findings. Effect 230 sizes were calculated as the ratio of the mean difference to the pooled standard deviation of the 231 difference. The magnitude of the ES was classed as trivial (<0.2), small (0.2-0.6), moderate 232 (0.6-1.2), large (1.2-2.0) and very large (≥ 2.0) based on previous guidelines (4).

233

234 **RESULTS**

235 *Participant characteristics.* Individuals with PP were older than both AB and TP (p < 0.01).

236 Compared to AB, sum of skinfolds and percentage body fat were greater in PP and TP ($p \le 1$

237 0.04), whilst fat mass was greater (p < 0.001) and fat free mass smaller (p = 0.04) in PP.

238

239 Thermoregulatory responses. No significant differences in T_{gi} between groups were observed

240 at the start (p = 0.18, AB: 37.22 (0.29)°C, PP: 36.91 (0.40)°C and TP: 37.23 (0.45)°C) or

during the 20 min stabilisation period (p = 0.08). The change in T_{gi} during the last 5 minutes

of the stabilisation period was not significantly different between groups (p = 0.26, AB: 0.03

243 $(0.03)^{\circ}$ C, PP: 0.06 $(0.06)^{\circ}$ C and TP: 0.05 $(0.03)^{\circ}$ C). Absolute T_{gi} at 65% RH was

244 significantly cooler in AB (37.43 (0.25)°C, p < 0.001, ES = 2.6) and PP (37.53 (0.45)°C, p = 0.001, ES = 2.6)

245 0.01, ES = 1.5) than in TP (38.16 (0.37)°C). The change in T_{gi} was smaller in AB than for TP

246 (p = 0.01, 95% CI = 0.07 to 0.47, ES = 1.5, Figure 2) from 30% to 65% RH. The critical RH

247 determined graphically for the groups are shown in Table 2.

248 Insert Ta

Insert Table 2 and Figure 2 here

No significiant differences in T_{sk} between groups were observed at the start (p = 0.91, AB: 34.34 (0.65)°C, PP: 34.27 (0.90)°C and TP: 34.14 (1.05)°C) or during the stabilisation period (p = 0.07). Mean skin temperature at 65% RH was significantly cooler in AB (36.25 (0.36)°C) than in PP (36.91 (0.56)°C, p = 0.05, ES = 1.3) and TP (37.45 (0.58)°C, p < 0.001, ES = 2.5). The change in T_{sk} was significantly smaller in AB compared to PP (p = 0.01, 95% CI = 0.14 to 0.98, ES = 1.5) and TP (p = 0.01, 95% CI = 0.29 to 1.03, ES = 2.0) across all RH stages (Figure 2).

256 There was a main effect of time at all individual skin temperature sites (all p < 0.001), with 257 responses shown in Figure 3. There were no differences between groups for the change in chest, 258 hand and foot skin temperature (all $\ge p = 0.07, \le ES = 0.4$) across all RH stages. The change 259 in forearm, upper back and abdomen skin temperature were smaller in AB and PP than TP (all 260 $p \le 0.02$, $\ge ES = 1.2$) across all RH stages. The change in upper arm skin temperature was 261 smaller in AB than TP across all RH stages (p = 0.01, ES = 1.5). The change in forehead skin 262 temperature was smaller in AB than TP from 45% to 65% RH (p = 0.04, ES = 0.2). The change 263 in thigh and calf skin temperatures were smaller in AB than both PP (p < 0.01, ES = 1.6) and 264 TP (p < 0.01, ES = 1.6 - 1.7) across all RH stages.

265

Insert Figure 3 here

266 No significant difference in HR was observed between groups at the start (p = 0.18; AB: 62 (7) 267 b·min⁻¹, PP: 74 (19) b·min⁻¹ and TP: 71 (4) b·min⁻¹), during the 20 min stabilisation period (p 268 = 0.16) or during the protocol (p = 0.43). The change in HR during the last 5 minutes of the 269 stabilisation period was not significantly different between groups (p = 0.33, AB: -5 (3) b·min⁻ ¹, PP: 0 (4) b·min⁻¹ and TP: -5 (10) b·min⁻¹). Heart rate at 65% RH was not significantly 270 271 different between groups, though, compared to AB (68 (10) b·min⁻¹), ES were moderate for PP 272 $(86 (26) \text{ b} \cdot \text{min}^{-1}, \text{p} = 0.16, \text{ES} = 0.9)$ and very large for TP (89 (8) $\text{b} \cdot \text{min}^{-1}, \text{p} = 0.09, \text{ES} = 2.3).$ 273 T_{gi} , T_{sk} , skin temperatures and HR all significantly increased over time (p < 0.001).

274

275 *Perceptual responses.* No significant differences were observed between groups for thermal 276 sensation or thermal comfort (p > 0.05). Participants became hotter and developed greater 277 thermal discomfort throughout (p < 0.001). Wetness sensation was significantly higher in AB 278 at 30-35% and 50-65% RH (p < 0.001) than TP and significantly increased over time (p <279 0.001).

280

Fluid balance. Urine specific gravity was not significantly different between groups at the start (p = 0.67) but was significantly greater in AB compared to PP (p = 0.02) and TP (p = 0.04) at the end of the protocol. PP and TP gained body mass compared to AB (p = 0.10) and AB and PP tended to consume more fluid than TP (p = 0.31), but neither were significant. Total mass loss and sweat rate were significantly greater in AB than PP (p < 0.001, ES = 1.4 - 1.7) and TP (p < 0.001, ES = 1.7 - 2.0, Table 3).

287

295

Insert Table 3 here

Heat balance parameters. Metabolic heat production was not significantly different over time (p = 0.46) or between groups (p = 0.22, AB: 123 (21) W, PP: 111 (15) W and TP: 103 (29)) (Table 4). Dry heat exchange (R + C) was significantly different between AB and TP (p =0.01). C_{res}, E_{res} (p = 0.17) and E_{req} (p = 0.79) were not significantly different between groups (Table 4). Evaporative cooling potential, based on observed sweat rates was significantly lower for PP and TP compared to AB (p < 0.01), and fell short of E_{req} for both PP and TP.

Insert Table 4 here

296 *Complete and incomplete lesion responses.* Figure 4 shows mean and individual responses for 297 the change in T_{gi} and T_{sk} , respectively. Statistical analysis was not conducted on this data due 298 to the small sample size.

299

Insert Figure 4 here

300 DISCUSSION

301 The hypothesis of this study was that critical relative humidity limits would differ between 302 groups, with AB having the highest critical limit, TP the lowest and PP in between, linked to 303 their respective areas of sensate skin. While the decision on the climate settings was based on 304 pilot work with a TP participant, both PP and TP participants in the actual experiment struggled 305 to attain heat balance from the start of the experiment. Thus, it is evident that the response of 306 the participant used in the pilot study was not representative of the groups studied; an 307 unfortunate reflection of the large variability in physiological responses in individuals with an 308 SCI. Nevertheless, the order of the groups in terms of their T_{gi} response was as expected. While 309 7 out of 8 AB showed stable T_{gi} at the start and a defined threshold where T_{gi} stability was lost, 310 only 3 out of 8 PP and none of TP achieved this. This result was directly linked to a shortfall 311 in evaporative cooling potential (Table 3) in PP and TP, compared to required evaporative 312 cooling (E_{req}).

313 Metabolic heat production is the primary determinant of E_{req} , hence the similar metabolic heat 314 production (and metabolic energy expenditure) between the three groups in the present study 315 infers similar values for Ereq. Yet neither PP nor TP attained a steady Tgi response (Figure 2), 316 and hence heat balance during the protocol. For instance, at 65% RH, the change in T_{gi} for PP 317 and TP was 0.29°C and 0.51°C greater than AB, respectively. For AB T_{gi} was stable, up until 318 a mean critical RH of 79% RH. The results therefore indicate that, evaporative capacity was 319 insufficient from the start for TP and at the limit for PP in the studied conditions where 320 evaporation was the primary pathway for heat dissipation.

The attenuation in evaporative heat loss in individuals with an SCI is further depicted by the greater change in T_{sk} and smaller total mass loss in PP and TP compared to AB. Both the change in thigh and calf skin temperature, i.e. skin sites below the lesion level, were significantly greater in PP and TP than AB throughout the protocol (Figure 3), contributing to the greater T_{sk} response. These results further support the notion that latent heat loss is greatly reduced and insufficient to attain heat balance at rest for TP and most PP in the absence of convective heat loss.

328

329 Body composition. Historically body fatness was considered an important parameter for 330 thermoregulatory response. Though it was later shown that fat percentage is only a relevant 331 predictor of individual T_{core} and sweating responses to exercise when cool climates are 332 considered, and skin blood flow is low (16–18). This has been confirmed more recently (7) 333 showing that heat production and E_{req} are the main driving factors in explaining most of the 334 variance in T_{core} and whole body sweat loss in the heat. Whether body fatness explains a similar 335 amount of variance in T_{gi} in individuals with an SCI is unclear. It could be argued that the 336 reduced skin blood flow to the body regions below the lesion level would make heat transfer 337 from core to skin more sensitive to the thickness of the fat layer insulation, similar to what 338 happens in AB in the cold. In the present study, given the close to isothermal conditions, this 339 would however not have affected outcomes. Individuals with an SCI, due to skeletal muscle 340 denervation and inactivity of their lower limbs, have adverse changes to their overall body 341 composition. These include a greater fat mass of their legs and trunk not only compared to their 342 upper limbs but also in comparison to AB (20, 39, 40). Hence a large proportion of fat mass in 343 individuals with an SCI is below the lesion level, which for these individuals are body regions 344 not considered to be an effective body surface area (area of skin that can partake in heat 345 dissipation). In relation to methodology, the Durnin and Wormsley four site method has been

346 shown to under-predict body fat percentage compared to dual energy x-ray absorptiometry in 347 wheelchair athletes by 4.2% (44). Thus, actual differences in body fat percentage between AB 348 and both PP and TP are likely to be greater than reported. Nevertheless, in the current study 349 the greater percentage of body fat of PP and TP compared to AB should have had minimal 350 influence on the amount of evaporative heat loss, while due to the chosen minimal temperature 351 difference between air and skin, a negligible effect on convective heat loss is expected.

352

353 Although PP were significantly older than both AB and TP, this is likely to have had a minimal 354 effect on the findings. Previous research has shown that the capacity to dissipate heat reduces 355 with age, with a decrease in evaporative heat loss of 4-11% in humid conditions (35°C, 65% 356 RH) and 4-6% in dry conditions (35°C, 25% RH) in 40-50 year olds compared to 20-30 year 357 olds (26). These findings are related to exercise in the stated conditions and are therefore likely to be even less in resting conditions. In addition, an individual's $\dot{V}O_{2max}/\dot{V}O_{2peak}$ is likely to 358 359 play a larger role regarding an individual's T_{core} and sweat response to a warm humid 360 environment than the individual's age (16, 17). Thus, in the current study despite PP being 361 significantly older than AB and TP, the actual difference in age between the groups is unlikely 362 to have a major influence on heat dissipation. The presence, level and completeness of an SCI 363 and the individual's cardiovascular fitness, which will correspond to the individual's lesion 364 level, i.e. lowest cardiovascular fitness for TP, is likely to have a much larger influence.

365

Lower body skin temperatures. In individuals with an SCI, T_{sk} is likely to mask regional skin
temperature differences, in particular skin temperatures above and below the lesion level (32).
The change in thigh and calf skin temperatures were greater in both PP and TP than AB, due
to the disrupted blood flow, vascular atrophy, lack of sweating response and skeletal muscle
denervation below the level of the lesion (19). In individuals with an SCI, thigh and calf skin

temperatures (28-31 °C) have been shown to be cooler at rest than the upper body (32-34°C)
and compared to AB (32, 38). Hence, the lower body may be a potential site for heat storage
in hot conditions (32), due to the combination of a reduced capacity to dissipate heat and cooler
initial skin temperatures, leading to a greater thermal gradient between the skin and
environment.

376

377 Upper body skin temperatures. For upper body skin temperatures of the upper back and forearm 378 in PP and TP, the magnitude of the change in skin temperature reflected the preservation of the 379 sweating capacity of these regions. Yet, large standard deviation in chest skin temperature 380 within SCI groups (Figure 2), potentially due to differences in lesion completeness, could have 381 masked a statistically significant finding. The chest skin temperature site is below the lesion 382 level for TP so one would expect a greater increase in chest skin temperature compared to AB 383 and PP. Compared to other regions of the torso, the chest has a lower regional sweat rate (37), 384 thus the sweat response of AB and PP may have had a lower evaporative cooling effect, leading 385 to a similar skin temperature for all three groups.

386

387 At the forehead, though the magnitude of the effect was small (ES = 0.2), the change in skin 388 temperature was significantly greater in TP than AB (Figure 3). Individuals with TP have a 389 small surface area of sensate skin and exhibit little to no sweat response above the lesion 390 level. Incomplete injuries and thus intact neural pathways may however lead to some 391 individuals still exhibiting a small sweat response. Nevertheless, given the resulting small 392 surface area of sensate skin this sweat response would not be large enough to provide 393 effective evaporative heat loss, in conditions where heat loss is solely dependent on the 394 evaporation of sweat, clearly demonstrated by this study.

395

397 Perceptual responses. In the able-bodied, thermal sensation is largely dictated by skin 398 temperature, independent of T_{core} (36). In the present study, despite a higher T_{sk} in PP and TP, 399 thermal sensation was not significantly different between the groups suggesting that PP and TP 400 may not be able to perceive the magnitude of thermal strain compared to AB. These results 401 imply that the role of skin temperature for reporting thermal sensation may be limited for 402 individuals with an SCI, in particular TP, as a result of the small body surface area of sensate 403 skin (2). For thermal comfort, T_{core} and T_{sk} have been reported to contribute equally in AB (11). 404 Despite similar thermal comfort scores, TP had a greater change in T_{gi} and T_{sk} suggesting they 405 should have been in greater thermal discomfort than AB. Alternatively, this finding may 406 suggest that their tolerance to thermal discomfort is in fact greater, though this cannot be 407 confirmed by the results of this study. Wetness sensation was lower in TP compared to AB and 408 PP, due to the small body surface area of sensate skin and minimal sweating capacity. The 409 upper body has a greater proportion of high sweat rate regions than the lower body (37). Thus, 410 despite a lower total mass loss and sweat rate in PP, perceived wetness of the sensate areas of 411 PP led to a similar wetness sensation score to AB.

412

413 Complete and incomplete lesion responses. As noted earlier, the large variance in 414 thermoregulatory responses in SCI is further complicated by the completeness of the lesion. 415 Individuals with incomplete lesions potentially having a greater amount of sensory information 416 and a greater body surface area available for sweating (43). The T_{gi} data grouped by lesion 417 completeness supports this notion (Figure A), yet individually there was disparity between the 418 T_{gi} of PP with incomplete lesions (all of which had a lesion below T8). Lesion completeness 419 did also not dictate which individuals with PP obtained a stable T_{gi}, i.e. prescriptive zone, and 420 a clear critical environmental limit. If complete lesions lead to a lower sweating capacity, one 421 would expect a complete lesion to have a greater T_{sk} response than incomplete lesions. Yet this was not the case in the present study, suggesting how completeness of the lesion influencesthermoregulatory responses is still not fully understood.

424 Limitations

425 Gastrointestinal temperature has been previously reported to demonstrate a temporal lag when used by able-bodied individuals (25, 41). Thus in the present study a lag in T_{gi} could 426 427 suggest the critical humidity limits reported could be higher than if oesophageal temperature 428 had been used. Yet if the lag was consistent between the three groups the differences in 429 evaporative heat loss between the groups would still be correct. A recent study by Au et al. 430 (3) investigated the comparison between oesophageal and T_{gi} during exercise in AB and 431 individuals with an SCI. Their results demonstrated that both methods provided similar 432 elevations in T_{core} in both AB and PP. Unfortunately there was no increase in T_{core} in TP in 433 their study, but this was most likely attributed to their lower heat production in TP of the 434 exercise undertaken. Therefore the study suggests that the lag is similar between AB and PP, 435 yet it is difficult to conclude whether a similar pattern is apparent for TP. However, a recent 436 study by Forsyth et al. (10) reported that the use of telemetric pills was appropriate for both 437 high and low level PP and TP during both exercise and recovery with a close relationship between T_{gi} and oesophageal temperature reported. In addition, practically due to the limited 438 439 ability to grip, TP (especially high level lesions) would also likely struggle to self-insert the 440 oesophageal probe.

441 Unfortunately, we did not measure the coverage of each wheelchair (seat and back rest) on
442 each participant, which is likely to differ depending on the level of support required.
443 However, it is important to note that for TP any sensate skin above the lesion is mostly nude
444 skin, so would not be affected by the coverage of the wheelchair or clothing. In PP, the
445 sensate skin areas of participants with the lowest lesion levels would be covered by the t –
446 shirt and back rest, whereas for participants with high level PP only half of their torso would

be active in convective and evaporative heat loss. In AB both the t-shirt, shorts, seat and back rest will cover skin surface areas active in convective and evaporative heat loss. Thus the coverage of clothing and the wheelchair is likely to have the greatest effect on AB and presents the best case scenario for this group in the current study. As a result of these differences in clothing and wheelchair coverage between and within groups, in our heat balance calculations we have not taken into account the amount of skin surface covered by the clothing and wheelchair.

454 As is evident from the results obtained, the chosen starting environmental conditions for TP 455 were too high to ensure the environment was compensable for all participants. In part this was 456 due to the pilot test results not matching the main experiment outcomes. A second factor is the 457 speed of the air flow in the chamber during the actual testing. The air flow of the climatic 458 chamber is usually 0.3 m/s given the settings used, however for this study it was recorded at 459 $0.12 \pm 0.07 \text{ m} \cdot \text{s}^{-1}$. Using the usual climatic chamber air flow and a maximum skin wettedness 460 value of 0.25 for TP, the starting environment would have been just compensable for these 461 individuals. Therefore upon reflection of the results a lower ambient temperature in the range 462 of 33 to 35°C for all trials would have ensured the starting environmental conditions were 463 compensable for all three groups, while still minimising convective heat losses.

464

465 *Conclusion.* The current study demonstrates that despite producing similar low levels of 466 metabolic heat and thus requiring the same low rate of evaporative cooling for heat balance, 467 TP had a heightened T_{gi} and T_{sk} response throughout the protocol compared to AB. Thus, even 468 at rest, in the absence of convective heat loss, evaporative heat loss in TP is not large enough 469 to balance the heat load at 37°C in an environment without solar radiation. Despite possessing 470 a greater sweating capacity and a smaller increase in T_{gi} than TP, the continual increase in both 471 T_{gi} and T_{sk} for a number of the PP participants and the too low evaporative cooling potential 472 observed, signifies evaporative heat loss capacity is also insufficient in PP, compared to AB.
473 Lastly, in the studied conditions, both PP and TP were unable to subjectively determine the
474 magnitude of their thermal strain and hence perceptual responses should not be relied upon for
475 this population group.

476

477

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482 **DISCLOSURES**

483 The authors declare no conflict of interest.

484 AUTHOR CONTRIBUTIONS

K.E.G., G.H., M.J.P and V.L.G.T conceived and designed the research. K.E.G performed
experiments, analysed the data and prepared figures. K.E.G., G.H., M.J.P and V.L.G.T
interpreted the results of the experiments and drafted, edited, revised and approved the final
manuscript.

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610		

Table.1 Participant characteristics for able-bodied individuals (n = 8), individuals with paraplegia (n = 8) and individuals with tetraplegia (n = 8)

7).

	Age (years)	Height (m)	Body mass (kg)	Sum of four skinfolds (mm) ^a	Body fat (%) ^b	Fat mass (kg)	Fat free mass (kg)	Body surface area (m ²) ^c	Lesion level (range)	Completeness of lesion ^d (number of participants)	Motor or sensory incompleteness (number of participants)
Able- bodied	28 (5)	1.88 (0.07)	75.99 (2.86)	31.5 (9.4)	14.4 (3.3)	11.0 (2.9)	65.0 (2.0)	1.96 (0.05)	n/a	n/a	
Paraplegia	45 (7) ^{§#}	1.77 (0.06)	77.41 (7.26)	61.8 (28.20) [§]	25.5 (7.3) [§]	17.5 (9.8) [§]	57.1 (4.6) [§]	1.94 (0.11)	T3-T12	Complete (5), Incomplete (3)	Sensory (1), Motor and sensory (2)
Tetraplegia	32 (3)	1.80 (0.09)	73.78 (12.24)	58.3 (13.7)*	21.5 (2.1)*	16.0 (3.8)	57.8 (8.6)	1.92 (0.20)	C5/6- C6/C7	Complete (2), Incomplete (5)	Sensory (3), Motor and sensory (2)

Data are mean values with SD in parentheses. All participants were male. \$ = significant difference between individuals with paraplegia and able-bodied individuals, # = significant difference between individuals with tetraplegia and individuals with paraplegia, *= significant difference between individuals with tetraplegia and able-bodied individuals. ^a Sum of skinfolds from biceps, triceps, subscapular and suprailliac sites. ^b Body fat percentage, was calculated using the Durin and Wormsley four site method (9). ^c Body surface area was calculated using the Dubois formula (8). ^d An individual with a complete injury has no motor and/or sensory function preserved in the lowest sacral segments of the spinal cord (S4-S5), whilst a motor or sensory incomplete injury refers to the preservation of motor and/or sensory function in the lowest sacral segments (S4-S5, (24))

Table 2 Mean critical relative humidity for able-bodied individuals and individuals with paraplegia. The number of participants a critical relative humidity could be determined for and the level and completeness of lesion for those individuals with a spinal cord injury is also shown.

Group (n)	Mean critical relative	Number of participants showing a	Lesion level/ Completeness of spinal cord
	humidity (%)	critical relative humidity limit	injury
Able-bodied (8)	77 (6)	7	
Paraplegia (8)	53 (14)	3	T4/5 complete, T8 incomplete sensory, T12 incomplete motor and sensory

Data are mean values with SD in parentheses. All participants were male.

	Able-bodied	Paraplegia	Tetraplegia
Urine specific gravity (pre)	1.018 (0.009)	1.016 (0.006)	1.019 (0.006)
Urine specific gravity (post)	1.025 (0.008)	1.015 (0.006) [§]	1.016 (0.003)*
Body mass loss (%)	0.06 (0.44)	-0.37 (0.39)	-0.19 (0.28)
Amount of fluid consumed (L)	0.41 (0.36)	0.46 (0.27)	0.24 (0.21)
Total mass loss (kg)	0.45 (0.05)	0.18 (0.11) [§]	0.11 (0.12)*
Sweat rate $(L \cdot h^{-1})$	0.22 (0.03)	0.09 (0.06)§	$0.06 (0.07)^{*}$
Potential cooling power (W)	147 (21)	63 (41) [§]	43 (46)*

Table 3 Fluid balance and evaporative cooling potential during the stepwise protocol for ablebodied individuals, individuals with paraplegia and individuals with tetraplegia.

Data are mean values with SD in parentheses. All participants were male., \$ = significant difference between individuals with paraplegia and able-bodied individuals, * = significant difference between individuals with tetraplegia and able-bodied individuals. Sweat rate was adjusted for respiratory mass losses (M_{res}). Percentage of body mass loss was calculated using the following formula ((Mass_{pre} - Mass_{post}) / Mass_{pre} · 100). Total mass loss was calculated using the following formula: ((Mass_{pre} - Mass_{post}) + fluid consumed).

	Able-bodied	Paraplegia	Tetraplegia
M (W)	123 (21)	111 (15)	103 (29)
Dry (W)	-2 (1)	-1 (2)	0 (2)*
$C_{res} + E_{res}$ (W)	6 (2)	5 (2)	5 (2)
E _{req} (W)	113 (20)	107 (17)	106 (29)

Table 4 Heat balance parameters during the stepwise protocol for able-bodied individuals, individuals with paraplegia and individuals with tetraplegia.

Data are mean values with SD in parentheses. All participants were male. M = metabolic energy expenditure/heat production, Dry = radiative (R) and convective heat exchange (C), $E_{res} =$ evaporative respiratory heat exchange, $C_{res} =$ convective respiratory heat exchange, $E_{req} =$ required rate of evaporative cooling. *= significant difference between individuals with tetraplegia and able-bodied individuals.

Figure 1 Two methods for removing participants from the climatic chamber. Participants were withdrawn from the climatic chamber after a clear inflection point in T_{gi} had been observed (critical RH limit, (26)), or T_{gi} increased by 1°C from the initial value upon entering the chamber. Note: To ensure a clear inflection in T_{gi} participants may not have been immediately removed from the climatic chamber following an initial rise in T_{gi} .



Figure 2 Change in gastrointestinal and mean skin temperature at rest in constant environmental temperature (37°C) and increasing humidity for ablebodied individuals (AB), and those with paraplegia (PP) and tetraplegia (TP). *= significant difference between individuals with tetraplegia and able-bodied individuals, $\S =$ significant difference between individuals with paraplegia and able-bodied individuals, † = statistical analysis was not conducted on these data, due to a reduced number of participants. The number of participants in each group for each time point are listed underneath the x axis. To calculate the predicted data, the difference between each time point (up till 65% RH) for each individual was calculated. The average differences for each time point were then added to the previous time point to estimate data points for 70-90% RH.



Figure 3 Change in upper arm, upper back, forehead, chest, calf and, thigh skin temperature at rest in constant environmental temperature (37°C) and increasing humidity for able-bodied individuals (AB), and those with paraplegia (PP) and tetraplegia (TP) upto 65% relative humidity. § = significant difference between individuals with paraplegia and able-bodied individuals, # = significant difference between individuals with tetraplegia and individuals with paraplegia, *= significant difference between individuals with tetraplegia and able-bodied individuals.



Figure 4 (A) The change in gastrointestinal and mean skin temperature for individuals with paraplegia (PP) and individuals with tetraplegia (TP) with complete and incomplete lesions compared to able-bodied individuals (AB). (B) Individual responses for the change in gastrointestinal and mean skin temperature for complete and incomplete lesions for PP and TP. Note: five individuals with paraplegia had complete lesions and three with incomplete lesions. Two individuals with tetraplegia had complete lesions and two with incomplete lesions

