A platform for screening abiotic/biotic interactions using indicator displacement assays

Monika Michaelis,^{1,2‡} Aneeqa Fayyaz,^{1‡} Mithun Parambath,^{1‡} Susan Koeppen,² Lucio Colombi Ciacchi,² Quentin S. Hanley,³ Carole C. Perry^{*1}

¹Biomolecular and Materials Interface Research Group, School of Science and Technology, Nottingham Trent University, Clifton Lane, Nottingham, UK NG11 8NS; ²University of Bremen, Hybrid Materials Interfaces Group, Faculty of Production Engineering, Bremen Center for Computational Material Science (BCCMS), Center for Environmental Research and Sustainable Technology (UFT) and MAPEX Centre for Materials and Processes, D-28359 Bremen; ³The Analytical Chemistry Research Group. School of Science and Technology, Nottingham Trent University, Clifton Lane, Nottingham, UK NG11 8NS

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ABSTRACT

This paper describes novel adaptations of optically sectioned planar format assays to screen compounds for their affinities to materials surfaces. The novel platform, which we name Optical sectioned Indicator Displacement Assays (O-IDA), makes use of displaceable dyes in a format adaptable to high-throughput multi-well plate technologies. We describe two approaches; the first being where the dye exhibits fluorescence in both the surface bound and unbound state and the second, where fluorescence is lost upon displacement of the dye from the surface. Half maximal inhibitory concentration (IC₅₀), binding affinity (K_i), and binding free energy (ΔG_{ads}) values can be extracted from the raw data. Representative biomolecules were tested for interactions with silica in aqueous environment and ZnO (0001)-Zn and (10-10) facets in a non-aqueous environment. We provide the first experimental values for both the binding of small molecules to silica and the facetdependent ZnO binding affinity of key amino acids associated with ZnO-specific oligopeptides. The specific data will be invaluable to those studying interactions at interfaces both experimentally and computationally. O-IDA provides a general framework for the high-throughput screening of molecules binding to materials surfaces, which has important applications in drug delivery, (bio-) catalysis, biosensing and biomaterials engineering.

* Corresponding author: carole.perry@ntu.ac.uk

Introduction

Interactions at the abiotic/biotic interface are of fundamental interest in medical devices, drug delivery and catalysis and have wide applications ranging from polypeptide adsorption,^{1–4} cell adhesion,^{5,6} biomaterials,^{7–10} and biosensors.^{11,12} Common methods for the experimental quantification of interactions at materials' surfaces include quartz crystal microbalance (QCM),¹³ surface plasmon resonance (SPR)¹⁴ or single molecule force spectroscopy (SMFS).¹⁵ These techniques take an indirect measure of the interactions and heavily rely on the models applied during data analysis. Furthermore, the experimental procedure and the associated analysis can be very time consuming. A direct measurement of binding enthalpies can be achieved using isothermal titration calorimetry¹⁶ but the method is limited to stable suspensions.

Indicator displacement assays^{17–19} provide measurements of interactions based on the direct observation of competitive binding between a reference compound and the analyte of interest to a given interaction site. Although they are used in drug discovery and high throughput screening, to the best of our knowledge, they have not previously been applied to screening of molecules that bind to abiotic material surfaces. Adapting this approach into the field of abiotic/biotic interactions would represent an important advance and could enable comprehensive screening of interactions at the analyte/material interface. Screenable displacement assays in a planar format²⁰ have been described for receptor ligand interaction studies and this approach can indeed be adapted to measure molecular interactions with abiotic/biotic surfaces, as we will prove in this paper.

We establish the novel approach using two representative functional oxides with important applications in nanotechnology and biomedicine. The first system is silica, for which knowledge of important binding interactions can lead to a deeper understanding of silica-based drug delivery systems,^{21,22} the synthesis of new materials for biomedical use²³ and processes such as biosilicification^{24,25} in mineralizing organisms.^{26–28} Advancements in this research area will have direct implications in material science, medicine and bio-nanotechnology. For this system we selected representative amino acids, a small polyamine²⁹ and a drug, ibuprofen, that is often used in model studies.^{30–32}

As a second system, we chose zinc oxide which is widely used in the form of crystals and nanoparticles for applications ranging from (photo-) catalysis,³³ mechanical actuators,³⁴ piezoelectric and optoelectronic devices³⁵ through to biomedical applications.³⁶ This versatility is triggered by the unique properties of ZnO, which is a semiconductor with a wide direct band gap and a high exciton binding energy.³⁷ The morphology-dependent properties of ZnO can be altered using biomolecules, which lead to a large variety of shapes with small variations in the preparation conditions. Within this framework, the biomineralization of ZnO with amino acids is of special interest.^{38–43} For the selection of amino acids (H, C, S, L, A and P), we refer to prior studies where the interaction of binding peptides with specific ZnO crystal planes has been investigated.^{43,44} Further, histidine and cysteine are well known to bind Zn²⁺ ions in zinc finger proteins^{45–48} and while histidine was found to be enriched in a phage display study for two common surfaces of ZnO, namely the zinc-terminated (0001) and the oxygen-terminated (000-1) polar surfaces,⁴⁴ cysteine is usually suppressed due to the impairment of phage infectivity.^{49,50}

This paper describes an approach to measure abiotic-biotic interactions which involves the combination of optically sectioned planar format assays (OSPFA) using confocal scanning laser microscopy (CSLM) and an indicator displacement assay (IDA) for screening of compounds binding to abiotic surfaces. The goal is to enable high throughput screening of molecule libraries to identify compounds with high materials binding affinity. Although our examples are two

functional oxides, silica and ZnO, the approaches introduced here are general and could be applied to a wide range of materials.

Materials and Methods

Silica: Hydrophilic silica surfaces were produced following a previously described protocol,^{51–53} a brief description is provided in the SI. CSLM experiments were conducted using 96 microwell glass bottom black plates (Nunc 164588). To determine the binding constant of the PDMPO dye ((LysoSensorTM yellow/blue DND-160, 1 mM in dimethyl sulfoxide), Life Technologies) to the silica surfaces, we measured the concentration-dependent adsorption behavior and the timedependent increase of the fluorescence intensity upon interaction with the substrate. To measure the binding of the compounds of interest to the silica surface the following protocol was adopted. 1 µM PDMPO ((LysoSensor[™] yellow/blue DND-160, 1 mM in dimethyl sulfoxide), Life Technologies) in 0.1 M phosphate buffer at pH 7.2 was applied and incubated (2 hrs at RT). The solution was then removed and replaced with test compounds at concentrations from 1 mM to 1 nM) followed by incubation (2 hrs at RT). The treated wells were then subjected to CSLM (Leica TCS SP5 with 405nm excitation of PDMPO) with detection of fluorescence between 480 nm and 600 nm along the z-axis. Instrumental parameters were: the numerical aperture (0.5 NA), objectives (Leica HCX PL Fluotar, 20×), pinhole size (84 µm) and step size of 0.5 µm, PMT gain (1107 V), offset (2.7 %) and laser intensity (77 %). If not stated otherwise, a minimum of three intensity curves were averaged for each inhibitor molecule concentration and normalized to the maximum intensities. All reagents used, aniline hydrochloride, ammonium persulfate, glutaric dialdehyde (50% v/v), amino acids (alanine, histidine and aspartic acid), lysozyme, tetramethyl

orthosilicate (TMOS), polyamine (spermine), hydrochloric acid, sodium hydroxide, ibuprofen, monobasic potassium phosphate monohydrate and dibasic potassium phosphate were obtained from Sigma-Aldrich.

Zinc oxide: Single-crystalline ZnO (0001)-Zn and (10-10) substrates (Crystal GmBH, Berlin, Germany) were fixed in a 96 microwell plate after 30 min cleaning treatment with an UV Ozone Cleaner (ProCleaner Plus, BioForce Nanosciences). To determine the binding constant of the FluoZin-1 Dye (F24181, Thermo Fisher) to the ZnO surfaces, we measured the concentrationdependent adsorption behavior and the time-dependent increase of the fluorescence intensity upon interaction with the ZnO (0001)-Zn and (10-10) substrates. Binding studies were initiated by adding 200 µl of 10 µM FluoZin-1 dye in methanol and incubating (2 hr) on a shaker at 30 rpm at room temperature. The dye-containing solution was removed and replaced with 200 µl methanol (control) or with 200 µl solutions (1 nM to 1 mM) containing test compounds (the amino acids, H, C, S, L, A and P, Sigma-Aldrich) and incubated (2 hr) using the same conditions as above. Note: all the ZnO interaction studies were performed in methanol to avoid the rapid dissolution of ZnO single crystalline substrates in aqueous media.⁵⁴ The substrates were measured using CSLM (Leica TCS SP5) using 496 nm excitation of FluoZin-1) with detection of fluorescence between 498 nm and 601 nm along the z-axis. Instrumental parameters were: the numerical aperture (0.5 NA), objectives (Leica HCX PL Fluotar, $10\times$), pinhole size (84 µm) and step size of 1 µm, PMT gain (1107 V), offset (2.7 %) and laser intensity (67 %). If not stated otherwise, a minimum of three intensity curves were averaged for each inhibitor molecule concentration and normalized to the maximum intensities.

Data fitting: The assay results were fitted using a modification of the generalized logistic function using commercially available software (Origin; OriginLab 2015) using a Levenberg-Marquardt

6

algorithm with a tolerance of 10^{-9} and maximum number of 400 iterations. The resulting curve is plotted along with the 95% confidence intervals and the 95% prediction intervals.

Theory

This study adapts two similar fluorescence-based indicator displacement assays.^{18,19} One is the optically sectioned planar format assay (OSPFA), which has been described previously for antibodies and receptors (Figure 1a and e). The other involves selection of the indicator such that fluorescence is lost upon displacement (Figure 1b and f). Choosing an indicator with high affinity and specificity towards the surface of interest under the desired solvent conditions is key for this assay. For instance, PDMPO is known to be relatively insensitive to the presence of different ions and ionic strength⁵⁵ and FluoZin-1 was developed for a cellular environment. These surface-bound assays are based on a two-step process: (i) the indicator is brought into contact with the surface where it binds reversibly (Figure 1 a and b) and (ii) a competitive molecule is added at increasing concentration (Figure 1 e and f) to test its ability to displace the indicator. If the test molecule causes the indicator to move from the surface into solution this response can be detected.^{18,19} For studies involving PDMPO as the indicator, PDMPO is found both bound to the surface and in bulk solution and the contributions of each have to be isolated from the observed spectral response. The approach to separate out the value of interest is described in the supplementary information and Supplementary Figure 1. The surface-bound contribution is the quantity of interest for subsequent EC₅₀ and IC₅₀ determinations.



Figure 1: Binding assays of the selected indicators (upper panel) and comparison of the optically sectioned planar format indicator displacement assay for silica and ZnO (lower panel). a) and e) Schematic representation of the interaction at the silica interface ('reduced' indicates a reduction in signal intensity) and b) and f) at the ZnO interface. c) and g) Model reactions and their equilibrium constants during the binding assay and the displacement assay, respectively. S corresponds to the number of binding sites on the surface, F denotes the fluorescent dye and M the molecule of interest d) Concentration-dependent increase of the normalized fluorescent thin layer intensity B/B_{max}, fitted by a modification of the generalized logistic function, leading to four fitting parameters including two asymptotes (A_1 , A_2), the slope m as well as the normalized fluorescent thin layer intensity B/B₀ fitted by a modification of the generalized logistic function, leading to four fitting parameters including the wo asymptotes (A_1 , A_2), the slope m as well as the concentration producing 50% of the maximal response (EC₅₀). h) Concentration-dependent decrease of the normalized fluorescent thin layer intensity B/B₀ fitted by a modification of the generalized logistic function, leading to four fitting parameters including the two asymptotes (A_1 , A_2), the slope n as well as the concentration producing 50% of the maximal response (EC₅₀).

The use of dyes like FluoZin-1^{56,57} simplifies the treatment as FluoZin-1 becomes brightly fluorescent when it binds to Zn^{2+} in solution or to the coordinated zinc species in the surface of the ZnO single crystals used in this study; however, it is non-fluorescent when displaced from zinc species by a test compound.⁵⁶ Thus one can simply use the optical response along the *z*-axis perpendicular to the surface to obtain intensity values which are used directly in equations 1 and

2 for the EC_{50} and IC_{50} determinations. The approach is adaptable to non-planar sample shapes; however, the planar shape is useful as it allows ZnO single crystals with specific orientation, in this case (0001)-Zn and (10-10) surfaces, to be assessed.

Binding affinities of the indicator. For the optically sectioned planar format indicator displacement assay (O-IDA), the interaction of the indicator, in our case the fluorescent dyes PDMPO and FluoZin-1, with the substrate, silica and ZnO, respectively, must be calculated based on a binding assay before we can elucidate the interaction of the inhibitor molecules. This binding assay describes the formation of the fluorescent dye layer (thin layer) on the substrate. Upon maximum coverage of the substrate with the indicator a saturation of the maximum fluorescence intensity is observed, and addition of further indicator molecules does not contribute to the measured thin layer intensity meaning it does not alter the binding equilibrium.

Calculation of EC₅₀. Here we consider EC_{50} as the concentration required to reach half saturation of the surface with indicator. The values are obtained by fitting the indicator/ dye concentration and the associated intensities to a logistic dose-response equation:

$$\frac{B}{B_{max}} = A_1 + \frac{A_2 - A_1}{1 + 10^{(x - \log x_0)m}} .$$
(1)

Plotting the fluorescence intensity B against the logarithm of the concentration x results in a sigmoidal shape for any value of the slope of the dose response curve m. A_1 and A_2 describe the asymptotes, x_0 corresponds to the sigmoid midpoint, which gives the EC₅₀ values as 10^{x_0} .

If fluorescence intensities are normalized to B_{max} , $A_2 = 1$ and in the case where there is no residual background, A_1 simplifies to 0. The surface specific binding constant K_F of the fluorescence dye depends on the slope, *m*, of the curves via $K_F = EC_{50}^m$. When m = 1, EC₅₀ would be equivalent to the dissociation constant of the fluorescence dye from the surface (K_F).

Indicator displacement assay: To perform the indicator displacement assay, we firstly remove the supernatant including the non-bonded indicator molecules and replace it with a solvent to access the fluorescence intensity after an incubation period. This fluorescence signal is the initial state for the following displacement assay and provides the reference intensity (B₀). For the displacement assay, the compound of interest is added in solution at different concentrations and the fluorescence signal is measured after an equilibration period and compared to the initial state. After full replacement of the dye, additional binding would not be detected for instance for the formation of multilayers.

Calculation of IC₅₀. During the indicator displacement assay, we access the so-called IC₅₀ value. Here, IC₅₀ is defined as the concentration required to displace 50% of the bound indicator molecules in the thin layer from the initial state. IC₅₀ is determined from the concentration dependent fluorescence of the indicator on the surface (c.f. Figure 1) and describes the potency of an assayed test compound. Modifying the generalized logistic function in equation 1 to account for a displacement by changing the sign of the exponent yields:

$$\frac{B}{B_0} = A_2 + \frac{A_1 - A_2}{1 + 10^{-(x - \log x_0)n}}$$
(2)

where the parameters are the same as in equation 1. Here the fits were simplified by applying a one-site competition curve, which is a dose response curve with a Hill slope *n* equal to 1. The IC₅₀ is then obtained from 10^{x_0} . Here, A_1 and A_2 can be used to account for residual fluorescence not treated already and to account for irreversible binding of the indicator dye.

Calculation of K_i. A quantity analogous to the inhibitory binding constant, K_i ,⁵⁸ can be defined for these assays. A range of approaches have been considered,^{58 59–62} however, the approach from Cheng,^{61,62} who highlighted the importance of the slope function, appears to be the most suitable for our treatment since it is obtained directly from the law of mass.^{61,62} This approach includes the slopes *n* and *m* for the antagonist (substrate of interest) and agonist (fluorescent dye), respectively, and gives:

$$K_{i} = \frac{IC_{50}^{n}}{1 + \left(\frac{[F]}{EC_{50}}\right)^{m}} = \frac{IC_{50}^{n}}{1 + \frac{[F]^{m}}{K_{F}}} \quad . \tag{3}$$

As noted before, in the current study we assume that n = 1.

Calculation of the free energy of fluorescent dye binding ΔG_F and adsorption ΔG_{ads} . The availability of an equilibrium dissociation constant for the binding of the fluorescent dye, K_F , allows for the calculation of the binding affinity following $\Delta G_F = -RT \ln(\bar{v}_s \cdot K_F)$ with \bar{v}_s being the partial molar volume of the solvent used,⁶³ in our cases $\bar{v}_s = 0.018 \ l \ mol^{-1}$ for the aqueous environment and $\bar{v}_s = 0.04046 \ l \ mol^{-1}$ for the methanol environment. The free energy of adsorption is calculated similarly, $\Delta G_{ads} = -RT \ln(\bar{v}_s \cdot K_i)$, with K_i being the inhibitory binding constant.

Results and discussion

The silica system is studied in aqueous media in accordance with previous binding studies¹ and conditions used for both studies of biomineralization and drug delivery. The ZnO system is studied in methanol to prevent dissolution⁵⁴ and to compare to conditions used in some bio-mineralization strategies.^{64,65} The usage of different solvent systems showcases the versatility of the approach.

Silica/PDMPO interaction in an optically sectioned planar format indicator displacement assay

Measurement of the binding of the PDMPO fluorescent dye in phosphate buffer to silica (Supplementary Figure 2) yield an EC₅₀ value of $1.75 \pm 0.27 \ \mu\text{M}$, $K_F = 0.01 \pm 0.02 \ \mu\text{M}$ and a binding energy $\Delta G_F = -13.28 \pm 0.12 \ \text{kcal mol}^{-1}$.

The assay system was then challenged with the amino acids alanine, histidine and aspartic acid, the polyamine spermine, and ibuprofen. These specific amino acids were chosen as they are commonly found in peptides that bind to silica.⁶⁶ A polyamine was selected as it has been found to be part of the post-translational modifications of proteins isolated from silicifying organisms such as some diatoms.^{67,68} It has also been shown to moderate silica formation *in vitro*.^{69,70} Ibuprofen was selected as an example of a commonly used hydrophobic drug which could serve as a test case for silica-based drug delivery systems that can control the release of drugs and deliver them to specific targets.

The dose response behaviour of the selected biomolecules are presented in Figure 2 (exemplarily for histidine) and in Supplementary Figure 3 (for all other systems). The calculated IC₅₀, K_i and ΔG_{ads} values are presented in Table 1. Of the compounds tested, ibuprofen had the strongest affinity for the silica surface and spermine the weakest. The binding energies covered the range from -12.82 to -9.39 kcal mol⁻¹ with the affinity of amino acids towards hydroxylated silica being: histidine>aspartic acid> alanine, this trend aligns with a computational study that studied the binding affinities of several amino acids to an amorphous hydroxylated silica surface with relatively different hydrophilicity performed under gas conditions.⁶⁸



Figure 2: Exemplar dose response curves from histidine a) with silica, b) with the (0001)-Zn, and c) with (10-10) ZnO single crystal surfaces.

Histidine's highest binding affinity to silica most likely includes interactions of the imidazole side chain interacting with silanol/siloxide groups on the silica surface as has been reported for peptides containing histidine.^{71,72} We propose that protonated N atoms of the imidazole ring may form direct H bonds with the silanol terminal group of the silica surface, in particular with deprotonated silanols that would be present at the pH of the experiment. Another contribution to binding will arise when the imidazole ring inserts flat into locally hydrophobic pockets while still forming hydrogen bonds with terminal OH groups. Both behaviours have been observed for peptide silica binding.^{71,72}

For the other two investigated amino acids, we obtain similar values for their binding affinity towards silica. With respect to the very different side functionalities, we would expect a common binding configuration *via* the amine group, which is known from molecular dynamics simulations on silica.^{71,73}

We note that computational studies of isolated amino acid binding to silica have only been performed on different surfaces of fully hydroxylated quartz in vacuum or for amino acid analogues on fully hydroxylated quartz in an aqueous environment; thus there is no directly comparable computational data available. Of the data that is available, computed adsorption enthalpies (ΔE_{ads}) for alanine and aspartic acid on the (10-10) surface of quartz range from ca. -17 to -20 kcal mol⁻¹.^{74,75} For studies of 'models of amino acids' (e.g. methane for alanine; methanol for serine; butylamine for lysine and acetic acid for glutamic acid) the values are all around the -1 to -2 kcal mol⁻¹ range.⁷⁶ For the investigated polyamine,⁷⁷ the interaction with silica will most probably be mediated by the amine groups, leading to a comparable binding affinity. Similarly, there are no computational data available for comparison.

Table 1: Binding affinities of selected biomolecules to silica surfaces. The standard error of the fitting for the IC50 values were propagated during the calculations.

Name		IC50	Ki	ΔG_{ads}
		(μΜ)	(μΜ)	(kcal mol ⁻¹)
	Alanine	6.17 ± 1.77	4.23 ± 1.30	-9.71 ± 0.18
Amino acids	Histidine	0.54 ± 0.11	0.37 ± 0.08	-11.15 ± 0.12
	Aspartic acid	3.43 ± 0.71	2.35 ± 0.52	-10.06 ± 0.13
Polyamine	Spermine	10.7 ± 2.0	7.33 ± 1.45	-9.39 ± 0.12
Drugs	Ibuprofen	0.032 ± 0.003	0.022 ± 0.003	-12.82 ± 0.08

In our experimental study, Ibuprofen was found to exhibit the highest binding affinity for silica amongst all studied binding partners, with $\Delta G_{ads} = -12.82 \pm 0.08$ kcal mol⁻¹. In recent density functional theory (DFT) simulations,^{32,78} interactions of ibuprofen with an hydroxylated silica surface were indeed shown to be exothermic and exergonic. Weak hydrogen-bonding between the carboxylic functionality of ibuprofen and OH surface groups of silica surface and dispersive attractions between the non-polar portion of ibuprofen and the surface were both found to be important,³² particularly in the presence of added water molecules.⁷⁸

ZnO/FluoZin indicator displacement assay

The facet-specific binding of FluoZin-1 to ZnO in methanol (Supplementary Figure 4 and Supplementary Table 1) indicates that binding is stronger to the polar terminated ZnO (0001)-Zn $((\Delta G_F = -16.32 \pm 0.03 \text{ kcal mol}^{-1})$ than to the mixed terminated (10-10) surface ($\Delta G_F = -14.58 \pm 0.05 \text{ kcal mol}^{-1}$). For the investigation of the binding affinities of amino acids we fitted the dose response behaviour with equation 2, similar to the Silica/PDMPO system (Figure 2, Supplementary Figure 5 and Supplementary Figure 6). The results are summarized in Table 2. The binding affinities of the amino acids to the (0001)-Zn surface can be ranked in the following order: histidine \geq proline > serine \geq cysteine > leucine \geq alanine. For the amino acid/(10-10) ZnO interface, the ranking of the amino acids leads to a slightly different order: proline \geq histidine > serine \geq cysteine > leucine.

The interaction of histidine and proline is characterized by very similar values of the binding free energy within our experimental setup (c.f. Table 2). While the interaction of Zn^{2+} ions in solution with histidine^{79–81} and within zinc finger proteins^{46,48,82–84} has been extensively

investigated, little is known about the interaction with proline. Biomineralization studies with amino acids support the strong influence of cysteine and histidine residues on the morphology of ZnO particles, while the influence of proline was less pronounced.^{85,86}

We hypothesize that the interaction of histidine and proline may take place through a qualitatively similar binding mode, namely via the nitrogen of the imidazole ring and the pyrrolidine group, respectively. However, the precise interaction patterns will very likely be determined by the local arrangement of the surface's terminal groups together with the exact protonation states of both the amino acids and the surface. Such protonation states in a pure methanol environment are not unambiguously accessible at this point and should be investigated carefully in future combined experimental/theoretical studies.

Table 2: Binding affinities of selected amino acids to the polar (0001)-Zn and the mixed terminated (10-10) surfaces of ZnO. The standard error of the fitting for the IC50 values were propagated during the calculations.

Name		IC50	Ki	ΔG_{ads}
		(μΜ)	(μΜ)	(kcal mol ⁻¹)
	(0001)-Zn	461 ± 23	6.94 ± 2.19	-8.94 ± 0.19
Alanine				
	(10-10)	153 ± 28	3.77 ± 0.98	-9.30 ± 0.15
	(0001)-Zn	53.2 ± 4.5	0.80 ± 0.26	-10.22 ± 0.19
Cysteine				
	(10-10)	62.6 ± 6.4	1.55 ± 0.33	-9.83 ± 0.13

	(0001)-Zn	0.39 ± 0.05	0.006 ± 0.002	-13.12 ± 0.20
Histidine				
	(10-10)	0.66 ± 0.06	0.016 ± 0.003	-12.53 ± 0.13
	(0001)-Zn	1.52 ± 0.07	0.023 ± 0.007	-12.33 ± 0.19
Proline	_			
	(10-10)	0.55 ± 0.06	0.014 ± 0.003	-12.63 ± 0.13
	(0001)-Zn	48.6 ± 4.7	0.73 ± 0.24	-10.27 ± 0.19
Serine				
	(10-10)	101 ± 5	2.49 ± 0.48	-9.55 ± 0.12
	(0001)-Zn	375 ± 28	5.64 ± 1.81	-9.06 ± 0.19
Leucine				
	(10-10)	231 ± 17	5.71 ±1.15	-9.05 ± 0.12

In agreement with previous research, we obtain similar binding affinities for the amino acids cysteine and serine.⁸⁷ Though a proton-transfer to the surface was proposed for the adsorption of cysteine on the (10-10) surface,⁸⁷ in agreement with the proposed interactions within zinc finger proteins, the interaction of cysteine and serine on this surface was attributed to the direct or indirect formation of hydrogen bonds including the carboxylate and side chain groups.⁸⁷ Presumably, the interaction of the aliphatic amino acids alanine⁸⁸ and leucine with the ZnO surfaces is *via* their c-terminal carboxylate groups alone, leading to the lowest binding affinities obtained in our experimental study.

Conclusions

This study reports the first measurements of small molecule interactions with silica and zinc oxide surfaces using optically sectioned indicator displacement assays (O-IDAs). As demonstrated using the ZnO system using methanol as the solvent, these O-IDAs are not restricted to aqueous systems or materials that are insoluble in an aqueous environment. They can be performed in any solvent and with any material provided a suitable dye is available and the system overall does not produce interfering fluorescence. Additionally, investigation of interaction kinetics may be possible provided that the interactions investigated happen on a timescale slower than the time of image acquisition in the confocal microscope.

The transfer of traditional indicator displacement assays to study the abiotic/biotic interface also requires us to keep in mind the underlying receptor occupancy theory with its assumptions.^{89–92} For a direct comparison, we do not know the number of accessible binding sites on our surface of interest, for instance due to surface protonation and system dynamics. In the framework of abiotic/biotic interactions, the maximum number of binding sites corresponds to the number that can be occupied by a known concentration of fluorescent dye. However, it is important to note that steric hindrance might prevent full occupancy. Further, during the displacement assay also non-indicator-occupied binding sites might be accessible and additionally not all analytes interact at the same binding site as the fluorescent dye due to the different chemistry involved. For instance, the dye FluoZin-1 binds to the zinc surface species, while some of the investigated amino acids will probably interact with the molecular adsorbed and/or dissociated water molecules present on the surface; the dye would in this case be displaced due to 'steric' considerations.

The O-IDA approach introduced here could be used similarly to the fluorescence-based indicator displacement assays in pharmacological screening since the method is convenient, robust, and scalable to high-throughput formats. In this form, O-IDAs could be of interest for assessing the

18

binding of medicinally relevant peptides or substrates for catalytic applications. This technique has advantages over quartz crystal microbalance (QCM) and surface plasmon resonance approaches by avoiding the issues associated with isolating the behaviour of molecules versus solvent/ions (QCM) and the need for a conductive surface (SPR). The only limitation of the O-IDA technique is the requirement for a fluorescent dye that has a specific interaction towards the abiotic surface of interest. A major advantage in comparison to the alternative approaches is the direct visualization of the adsorption events, which allows for quality control judgements regarding the homogeneity and spatial distributions of the response.

ASSOCIATED CONTENT

Supporting Information.

The following files are available free of charge:

Synthesis of the functionalised silica surfaces; Overview of the Silica/PDMPO interaction in a planar format indicator assay; Characterization of the fluorescent dye PDMPO; O-IDA results for amino acids, ibuprofen and spermine on Silica using PDMPO; Characterization of the fluorescent dye FluoZin-1; Binding affinity of FluoZin-1 towards ZnO (0001)-Zn and (10-10); O-IDA results for amino acids on ZnO (0001)-Zn using FluoZin-1; O-IDA results for amino acids on ZnO (10-10) using FluoZin-1.

AUTHOR INFORMATION

Corresponding Author

* carole.perry@ntu.ac.uk,

Author Contributions

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ABBREVIATIONS

CSLM: Confocal scanning laser microscopy; IDA: indicator displacement assay; OSPFA: optically sectioned planar format assay; SPR: surface plasmon resonance; QCM: quartz crystal microbalance

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